

High resolution extended depth of field microscopy using wavefront coding

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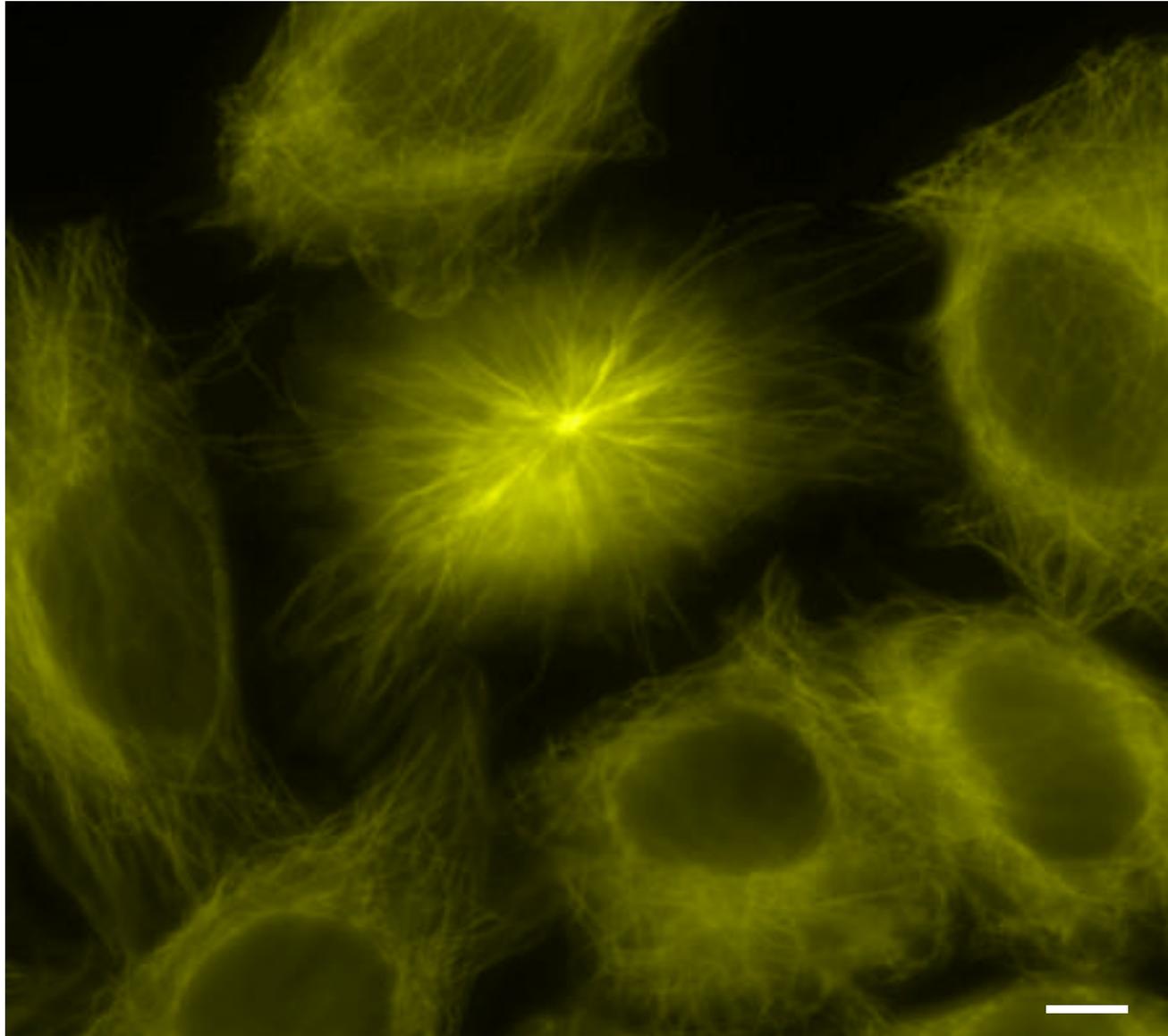
The Problem:

For **3D real-time fluorescence imaging** of live-cell dynamics and *in vivo* processes,

confocal and **widefield** (deconvolution) microscopes are often **too slow**,

because they require **sequential acquisition** of many planes of focus to build up a 3D image.

Standard Fluorescence

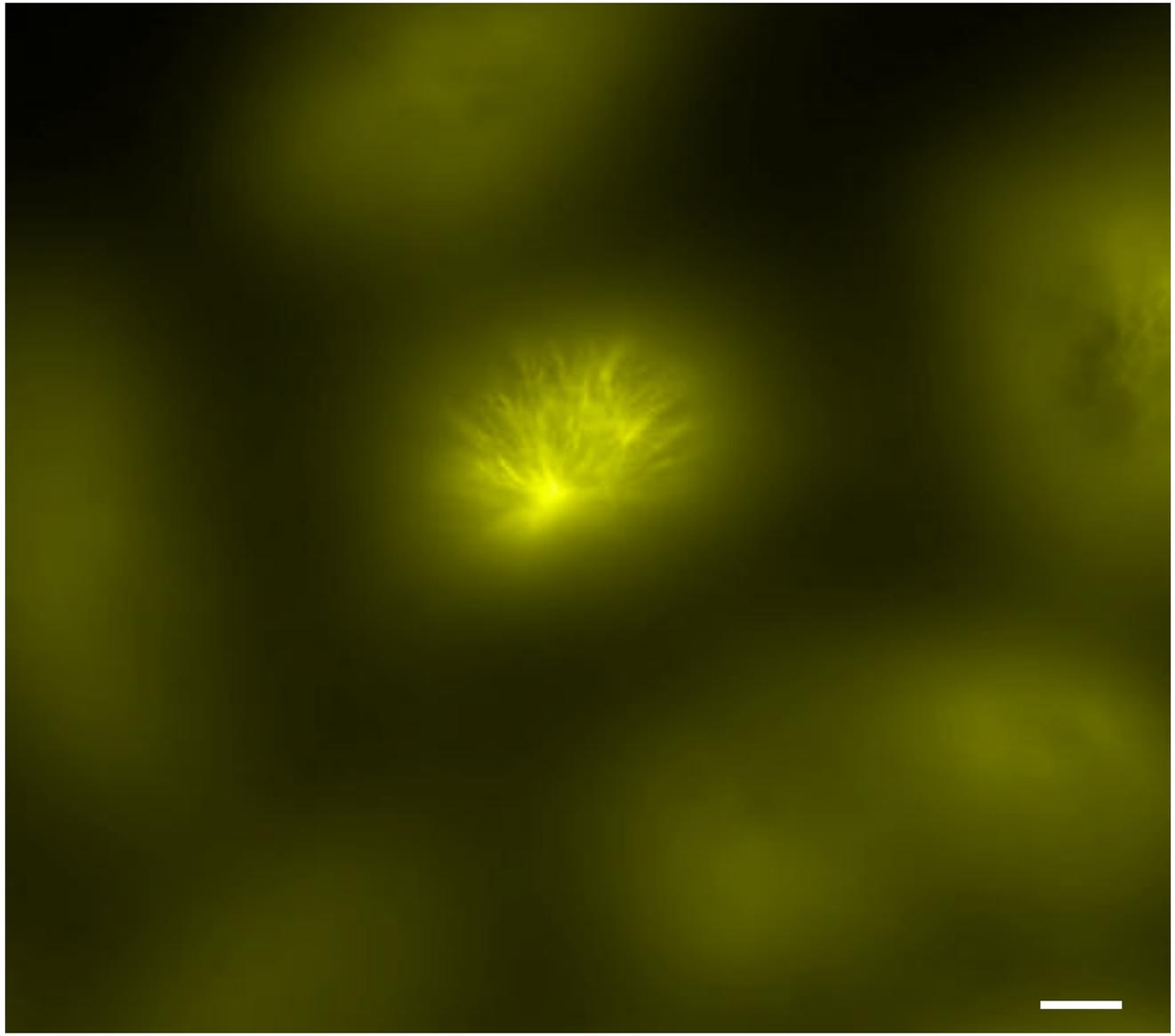


Specimen:
human HeLa
cancer cells,
imaged with
40x 1.3 NA oil
lens.

Focus at 1 μ m depth

scale = 6 μ m

Standard Fluorescence



Focus at 7 μ m depth

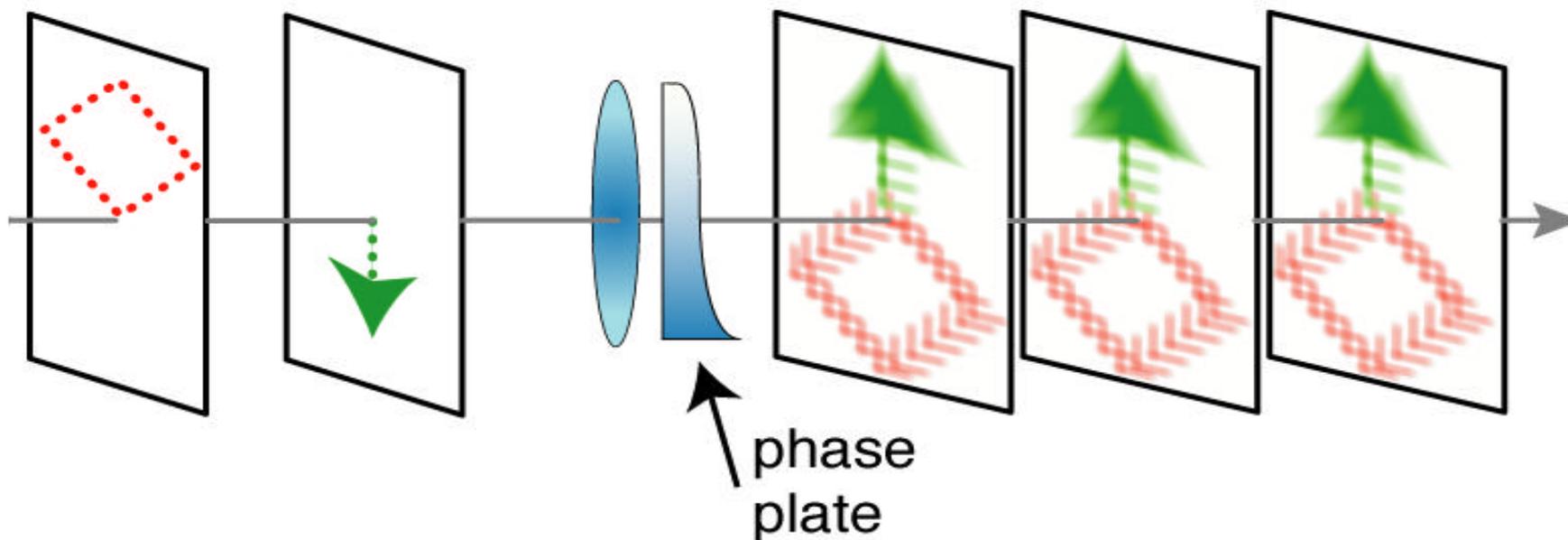
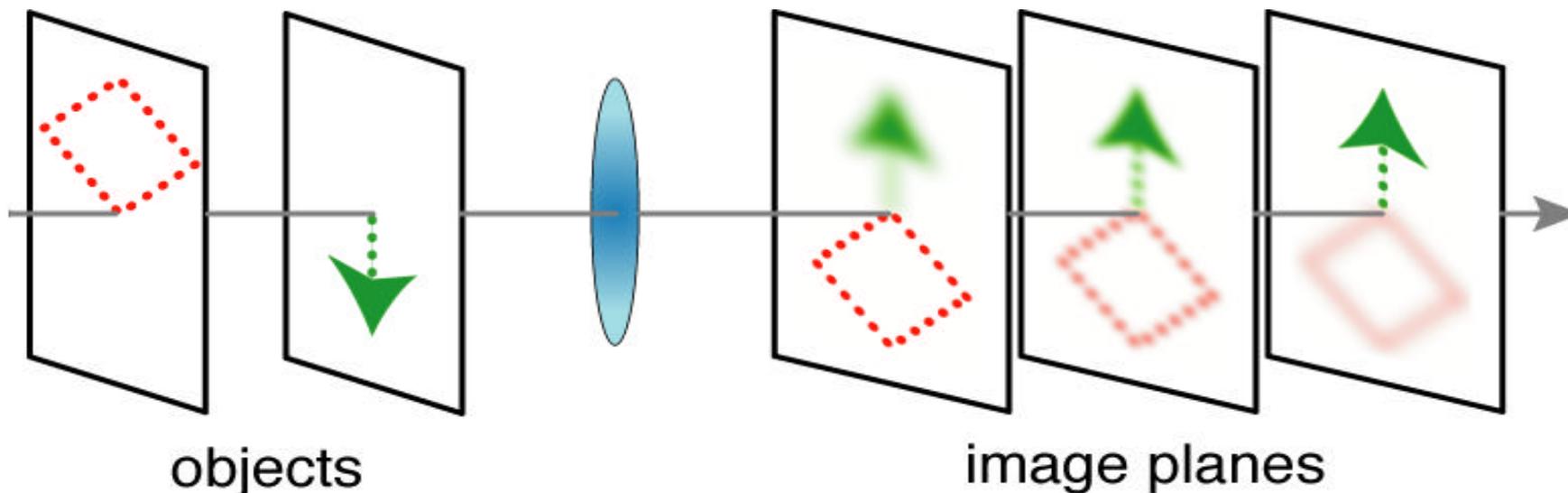
scale = 6 μ m

Solution: Extend the Depth of Field

Our high-speed EDF fluorescence microscope:

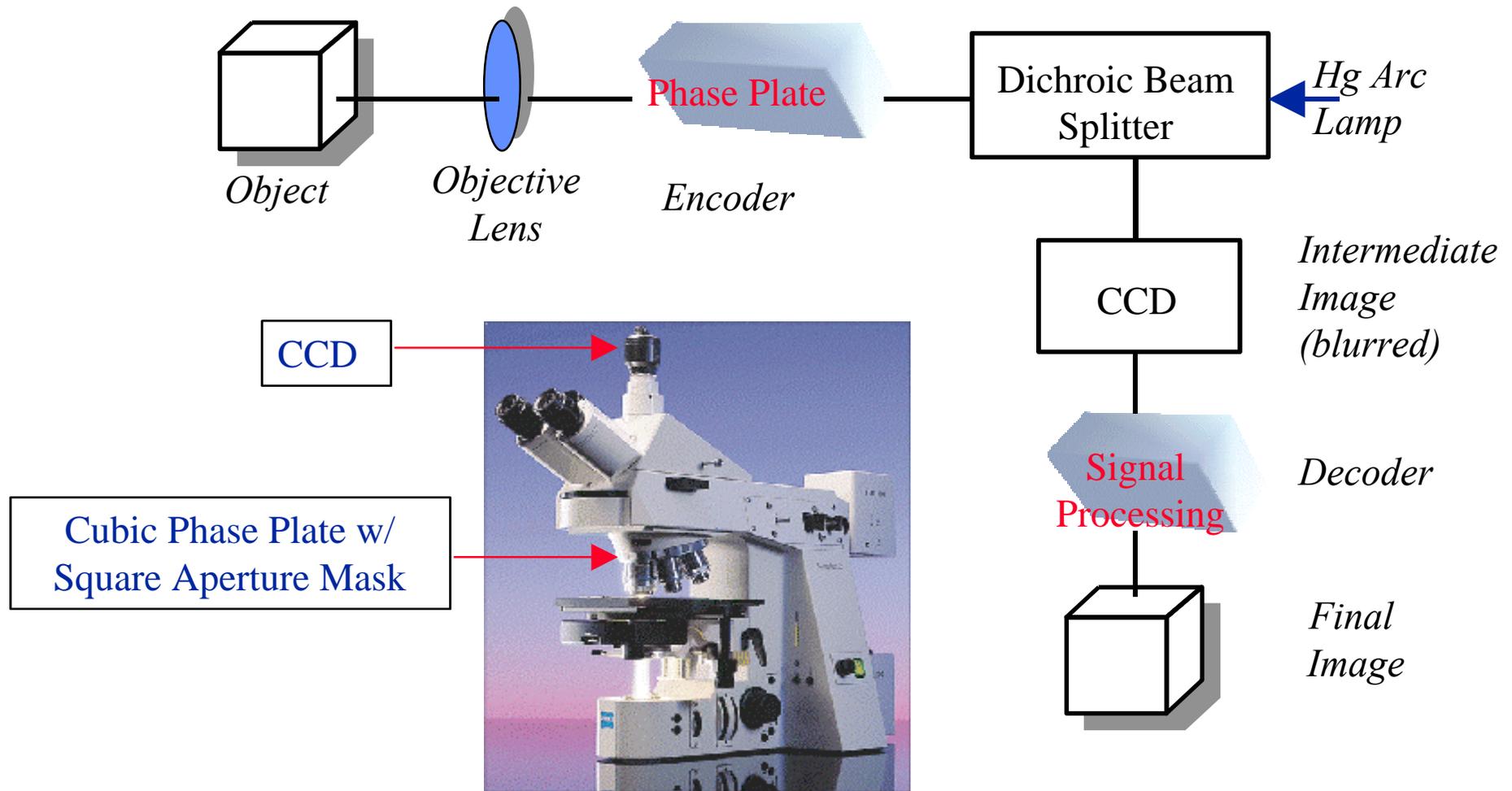
- * uses only a **single exposure** on a CCD
- * followed by a **single-step digital filter**, which can run at video rates
- * maintains **high NA resolution**, the tradeoff is a drop in signal to noise
- * may also reduce **photo-bleaching**

Normal optical system (limited depth-of-focus)



Wavefront coded system (uniformly blurred)

Diagram of EDF Optical/Digital System

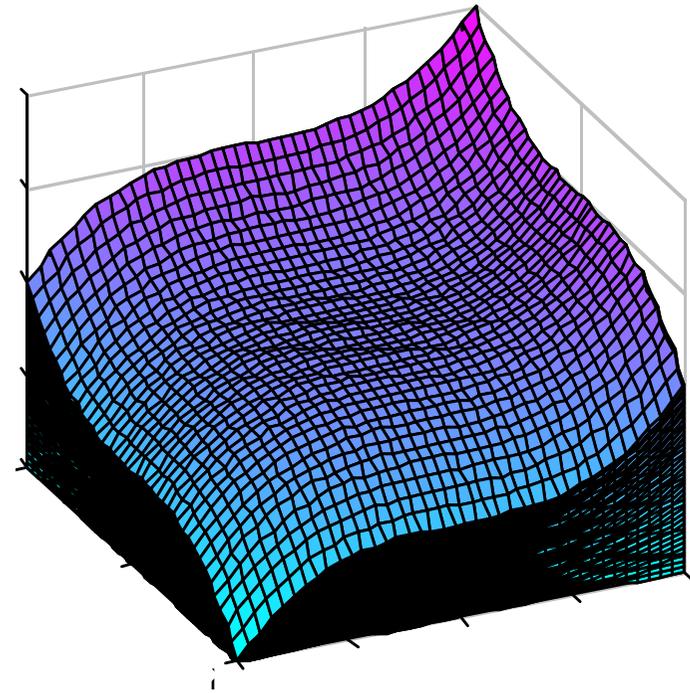


Cubic Phase Plate

The special *cubic phase plate* (CPP) has thickness corresponding to this 2-D function of spatial position:

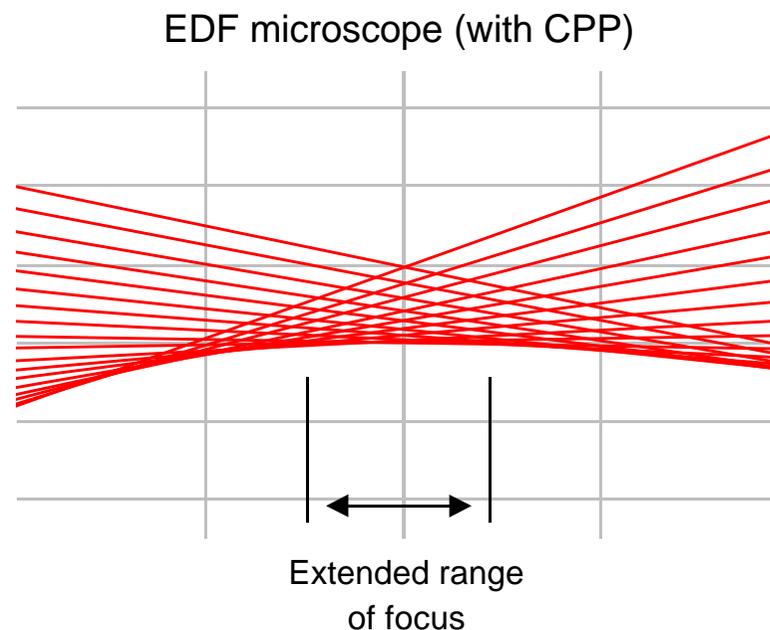
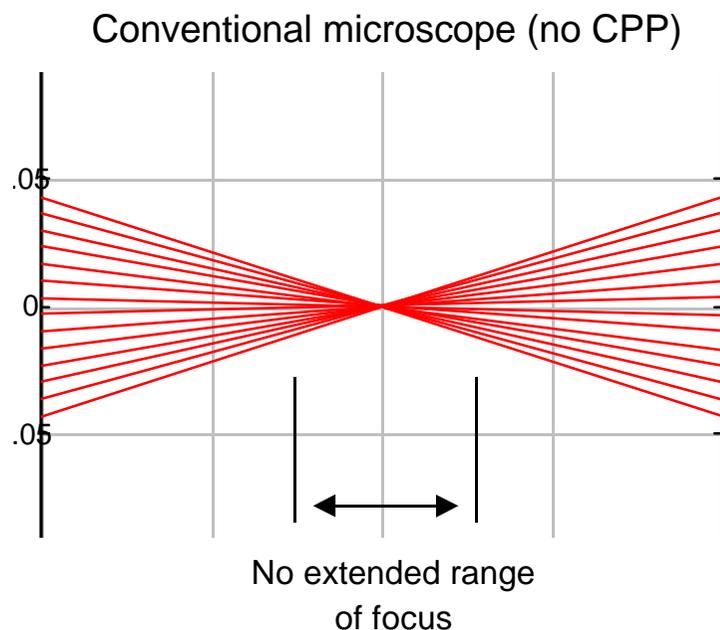
$$P(x, y) = a(x^3 + y^3)$$

The phase plate function “encodes” the wavefront, allowing for simple post-processing.



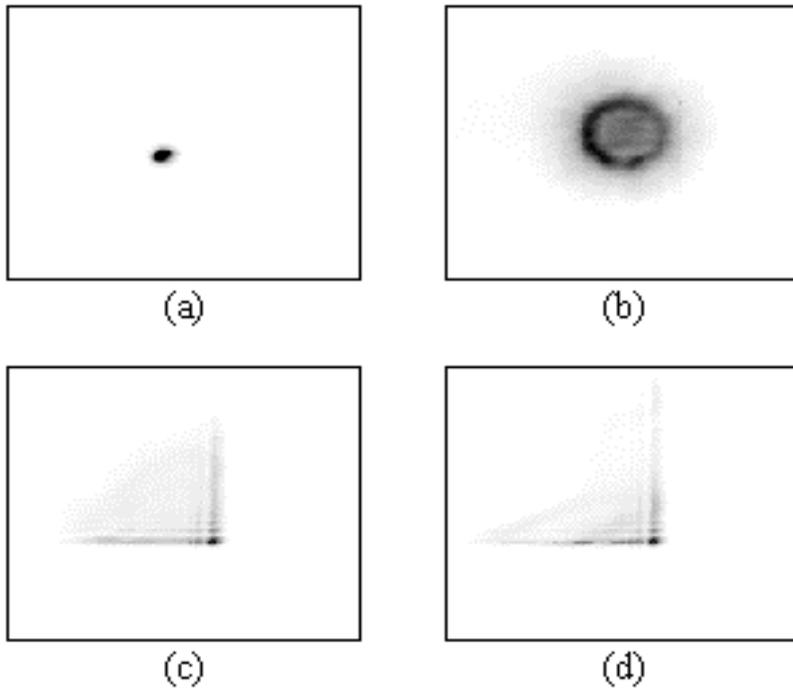
Cubic Phase Plate
Phase Plot

Conventional Lens vs Cubic Phase Plate (CPP) Ray Traces



With the addition of a CPP, **focus invariance** is extended along the z axis by an amount determined by the properties of the CPP and the lens numerical aperture.

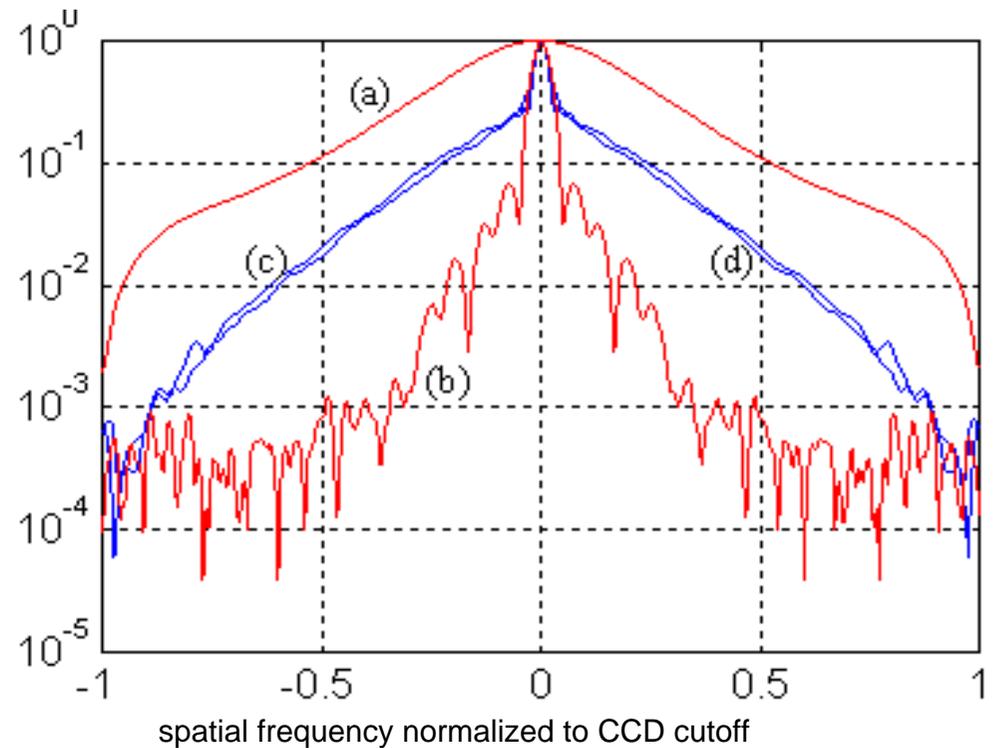
Focus Invariance: Point Spread and Modulation Transfer Functions EDF in a fluorescence microscope



Z = 0 μ m

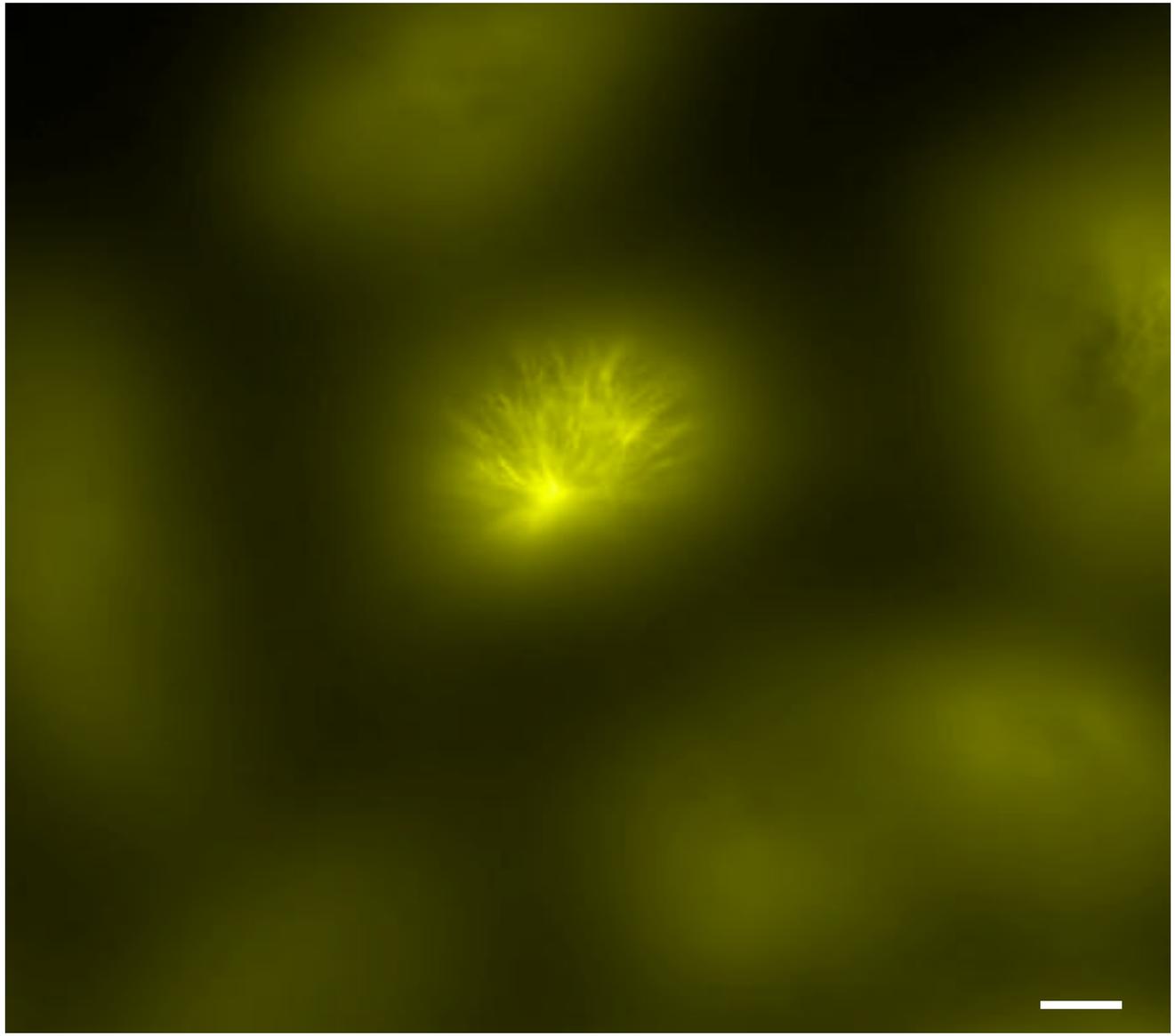
Z = 5 μ m

Standard (a, b) vs.
Cubic Phase Plate (c, d) PSFs



Standard vs. Cubic Phase
Plate MTFs

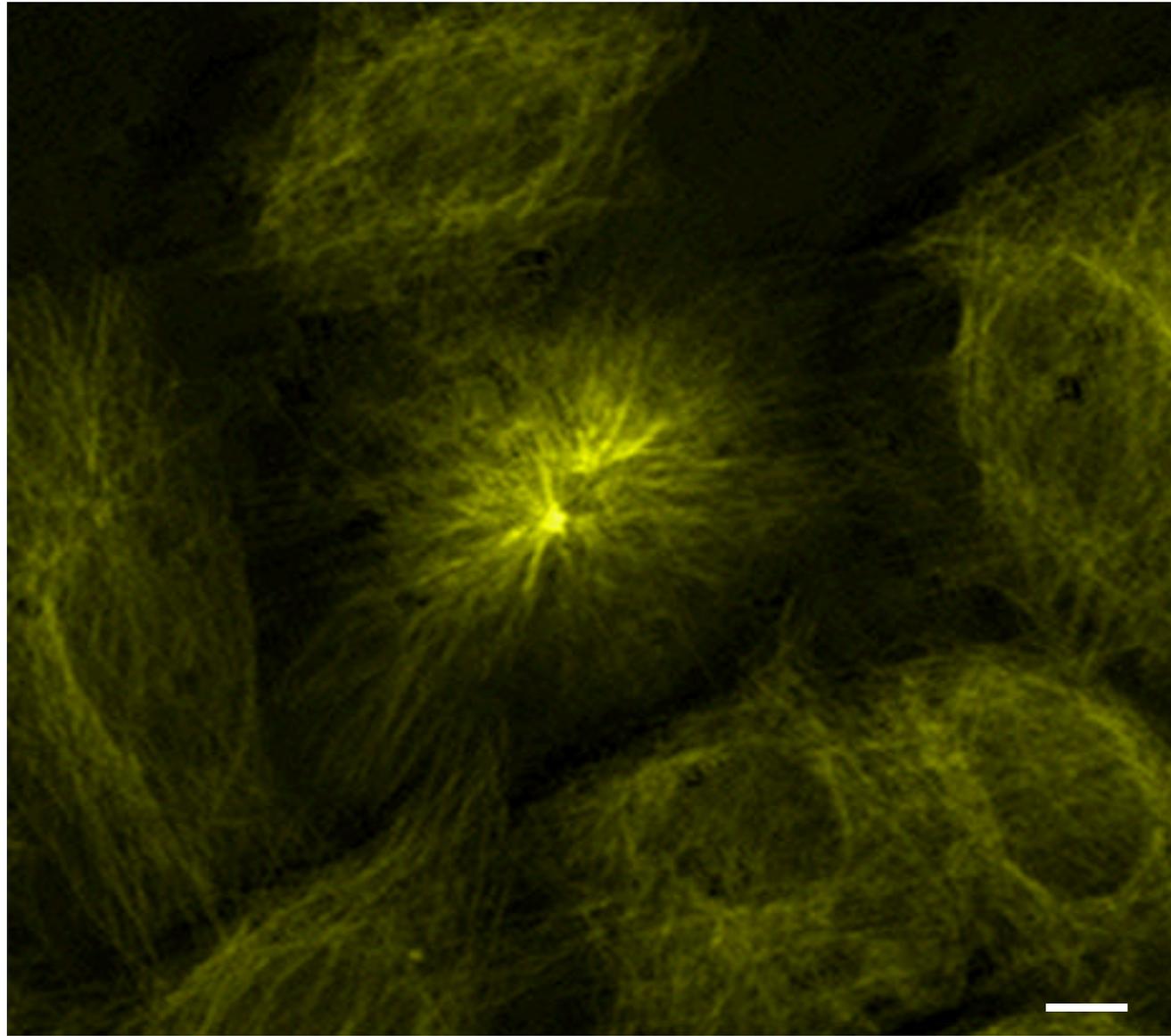
Standard Fluorescence



Focus at 7 μ m depth

scale = 6 μ m

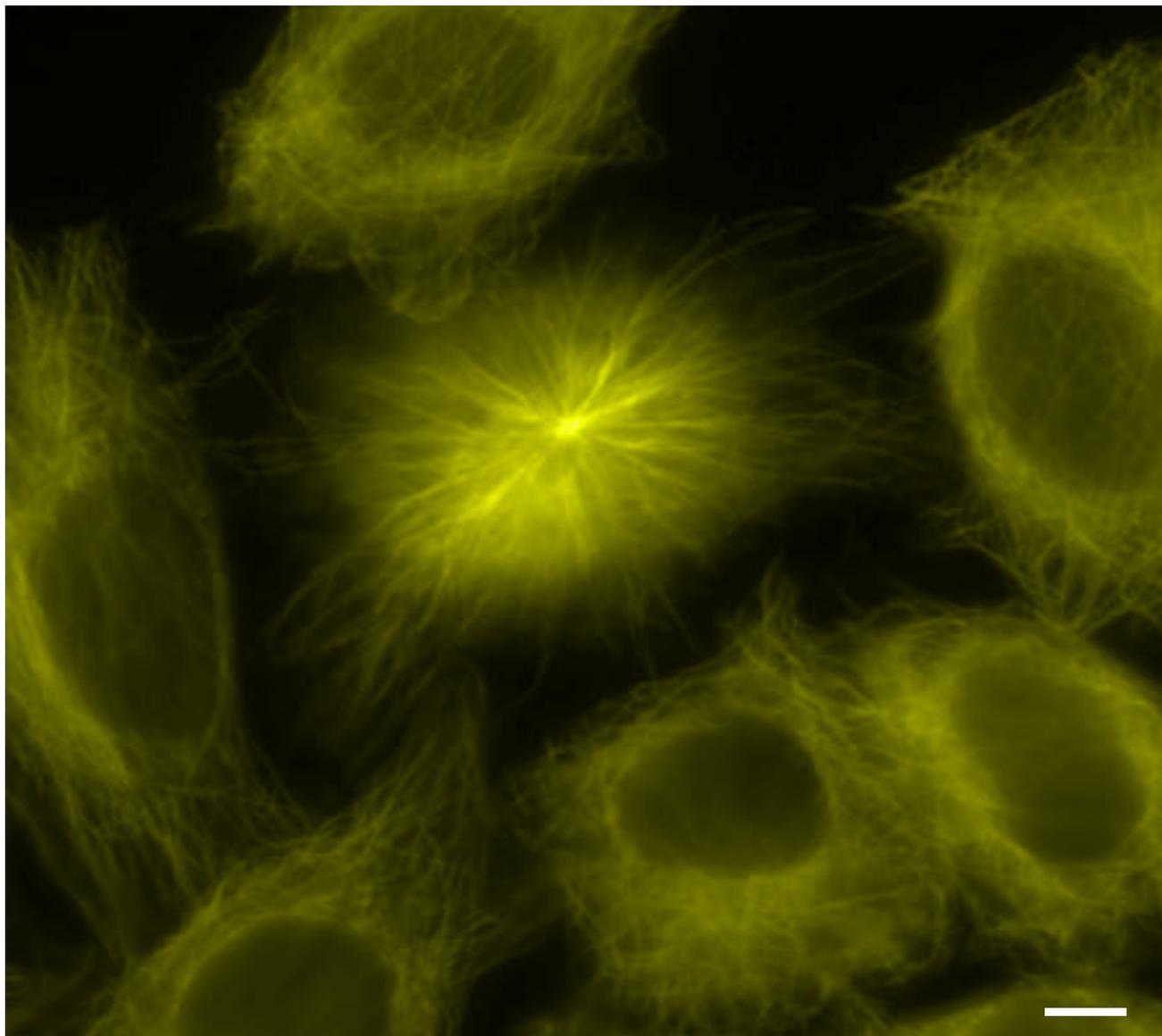
New EDF Fluorescence



Focus at 7 μ m depth

scale = 6 μ m

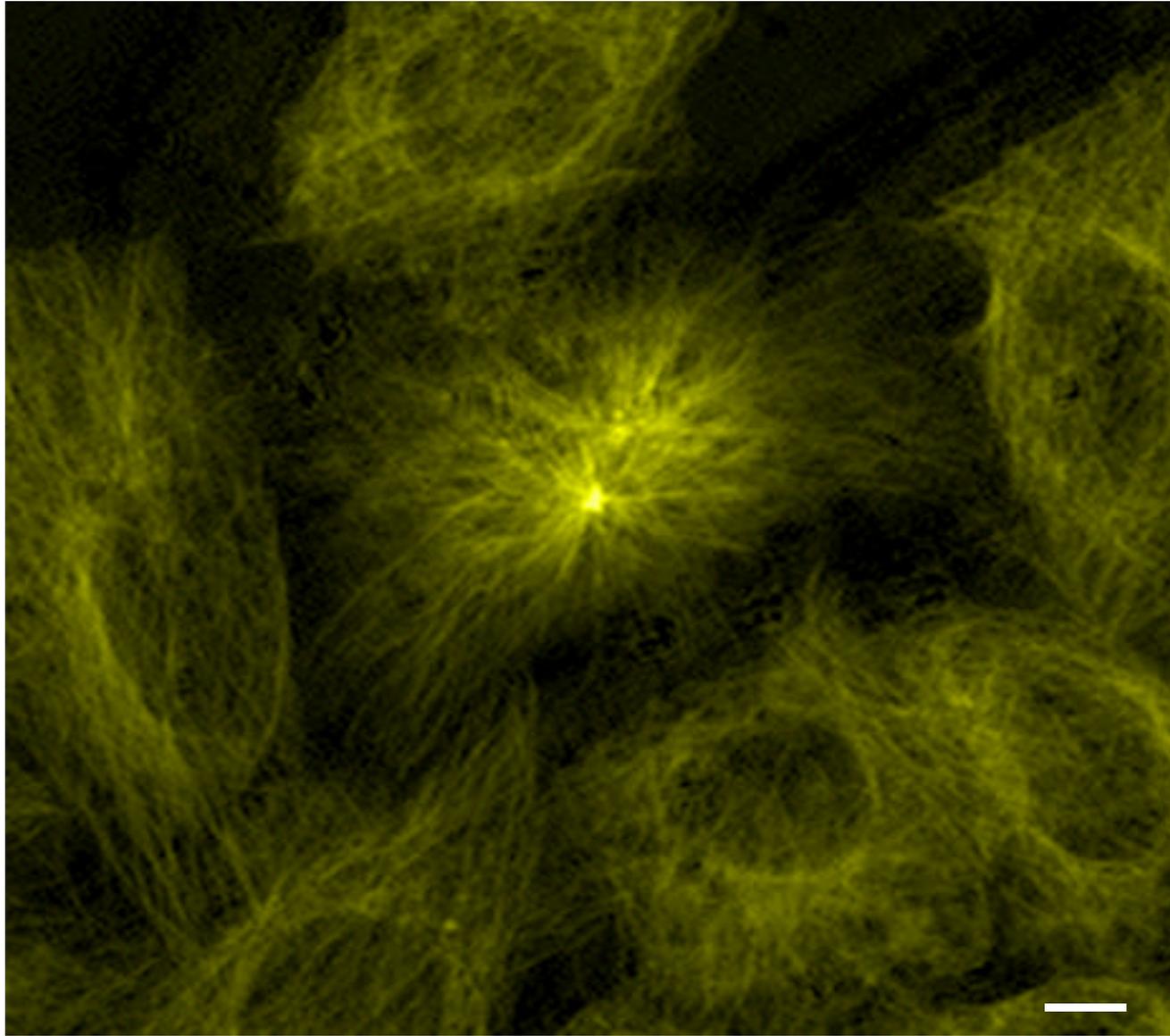
Standard Fluorescence



Focus at 1 μ m depth

scale = 6 μ m

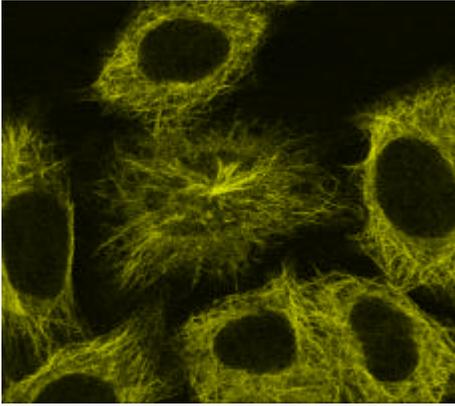
New EDF Fluorescence



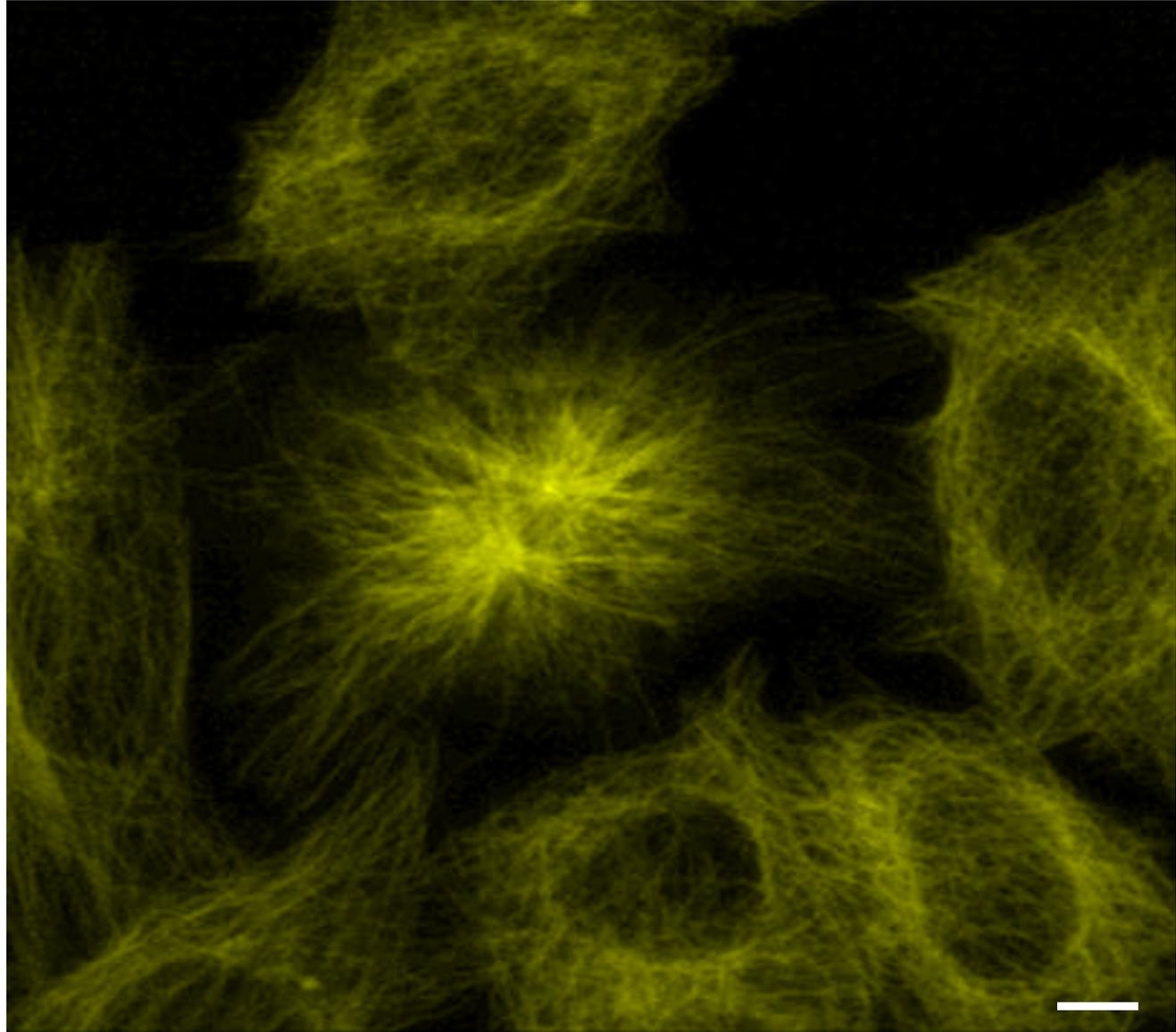
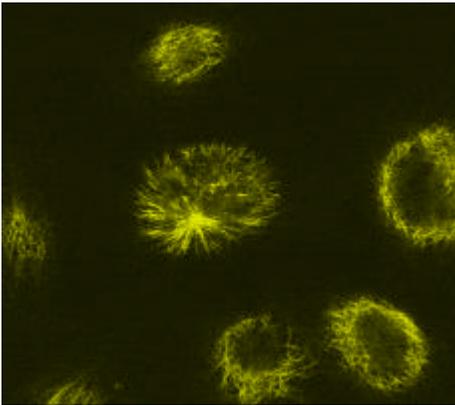
Focus at 1 μ m depth

scale = 6 μ m

Confocal Fluorescence



24 planes of focus at
0.5 μ m steps,
averaged

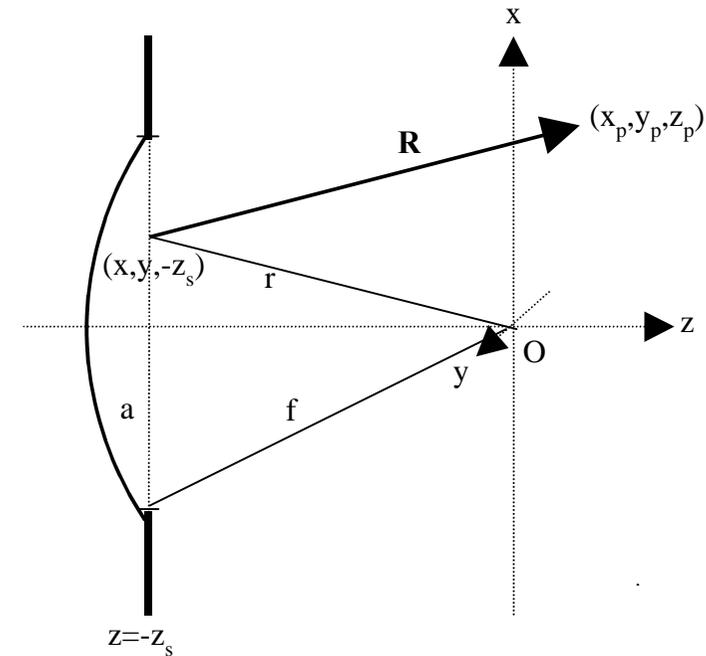


This took 20 times longer to acquire than our EDF images.

High Numerical Aperture Model

Previous work on wavefront coding has used the paraxial approximation. Here we simulate the system at high numerical aperture using the Rayleigh-Sommerfeld diffraction formula.

The field E is calculated by integrating across a square aperture.



$$E(x_p, y_p, z_p) = \int_{-a}^a \int_{-a}^a \exp(ik\varphi(x, y)) \frac{\exp(ik(R - r))}{rR} \frac{z_p + f}{R} dx dy$$

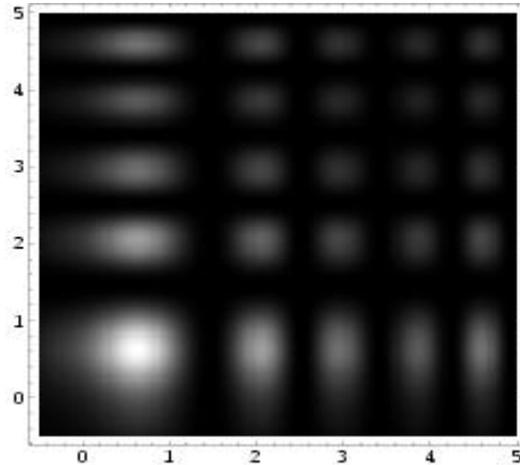
Where the cubic phase function is given by:

$$\varphi(x, y) = C(x^3 + y^3)$$

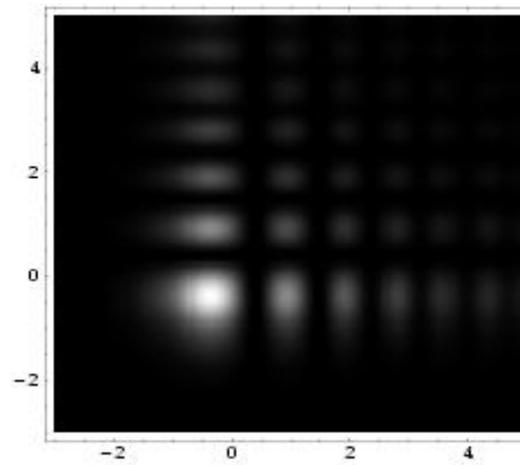
Theoretical Point Spread Functions

Paraxial
Approx.

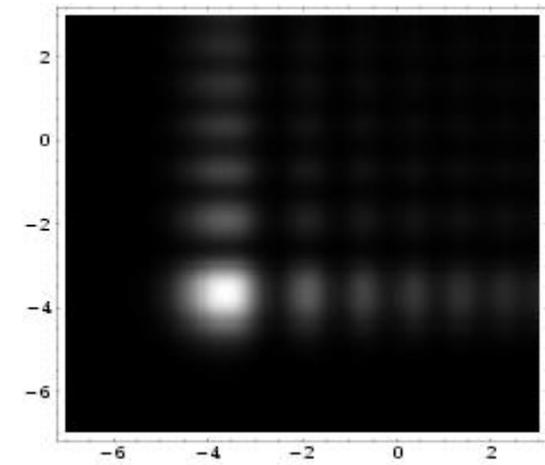
$z=0\mu\text{m}$



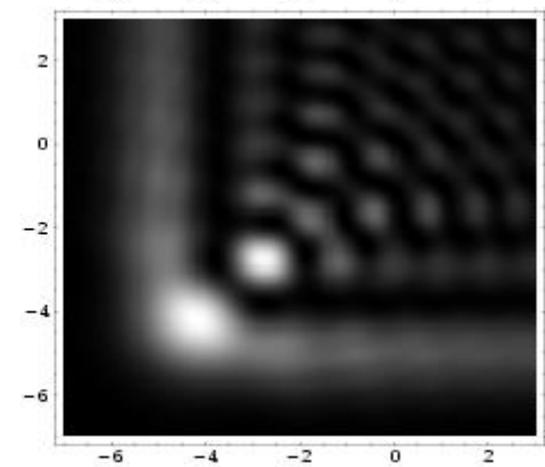
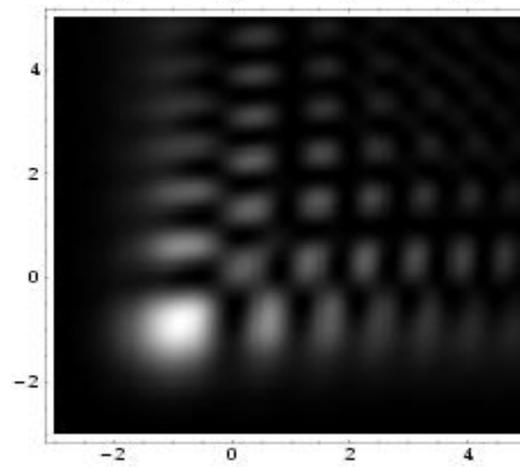
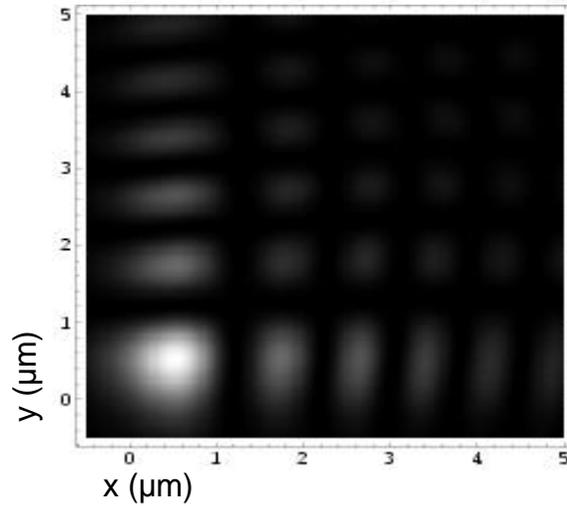
$Z=10\mu\text{m}$



$z=20\mu\text{m}$



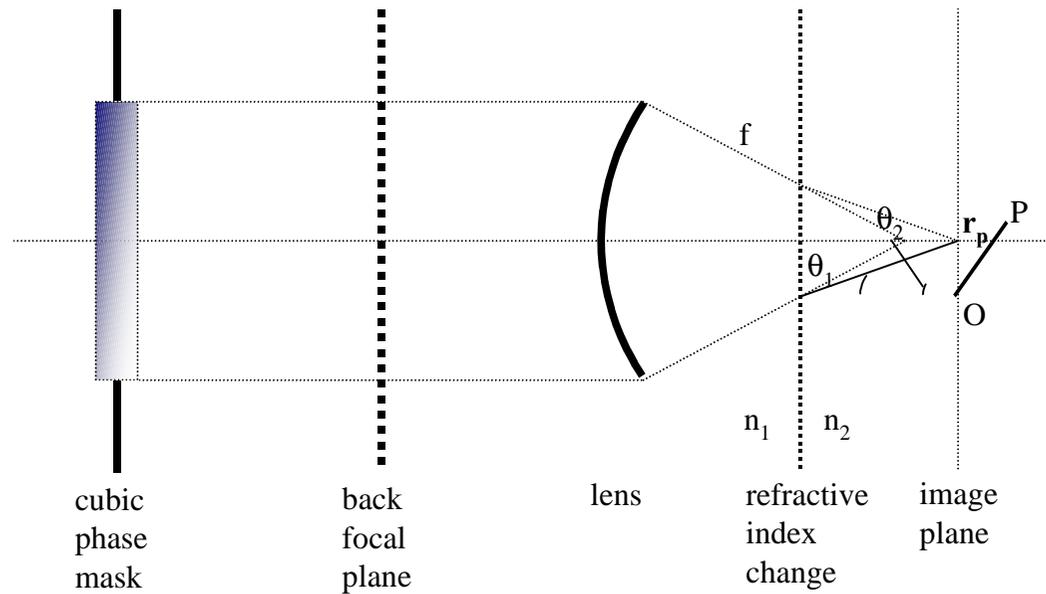
High NA



Simulating a 40x 1.3 NA oil lens, as used for the experimental images.

What Next for the Model?

- * Take better measurements of the high NA PSF to compare with theory.
- * Simulate the effects of other useful phase mask functions.
- * Add a change in refractive index - typically producing spherical aberration.



Conclusion:

Wavefront coding is a new approach to 3D fluorescence microscopy and to optical design in general. Instead of avoiding aberrations, we exploit them.

The system is inexpensive because it requires only small modifications to a standard fluorescence microscope.

This opens the way for new studies of a wide range of live-cell dynamics.